

Parallel proton CT image reconstruction

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Motivation and role of proton imaging

- Nowadays the importance of the proton therapy is increasing
⇒ more and more motivation to improve the technology
- The use of proton CT images is a promising direction
⇒ lower inaccuracy in RSP measurement
⇒ decreased safety zone around the tumour
- A pCT image measures the relative stopping power (RSP) distribution of the patient



Bergen pCT collaboration

- Goal: reach the clinical research with a pCT prototype
- Apply monolithic active pixel sensors (MAPS)
- Use pencil beam for imaging
- Measure 10^6 proton / second
- Reach $< 1\%$ RSP error

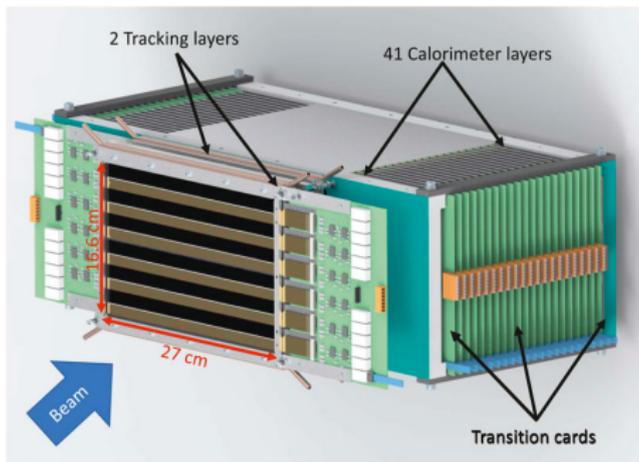


Image reconstruction – a large linear problem

The image reconstruction is a large and sparse linear problem:

$$\mathbf{y} = \mathbf{A} \mathbf{x} ,$$

where:

- \mathbf{y} is the measured data
- \mathbf{x} is the vector of voxels
- \mathbf{A} is the system matrix, contains the interaction coefficients
 - practically the path length of protons in the voxel
 - can have 10^{12} non zero element – about 12 Tbyte
 - ⇒ on the fly calculation of the element instead of store them
 - matrix element become a function: $A_{i,j} \Rightarrow A(i,j)$

Parallelization – important parameters

Hardware:

- 4 piece of Nvidia 1080Ti
- computer capability: 6.1
- CUDA version: 11.2

Parameters:

- N : the number of protons $\sim 10^9$
- M : the number of voxels $\sim 10^7$
- L : the typical number of interaction of a proton $\sim 10^3$
- T : the number of GPU treads $\sim 10^4$
- S : the number of SMs $\sim 10^2$
- TS : tread per SM – 128 \ 256 \ 512

Main aspects

- Minimize the num. of calculations of the same matrix element
- Read only a subset of proton histories at the same time
⇒ the memory use is independent of input data size
- Parallelize the problem in an efficient way
- Optimized for the given hardware
- Minimize CPU usage
- Minimize data transfer between CPU and GPU

Image reconstruction – Richardson – Lucy algorithm

- Originally introduced for astrophysics application
- It is a fixed point iteration for large and sparse linear problems
- Initialization: arbitrary positive vector
- Init: unit vector or precalculated approximate solution

The formula for the i^{th} element of the next image vector:

$$x_i^{k+1} = x_i^k \frac{1}{\sum_j A_{i,j}} \sum_j \frac{y_j}{\sum_l A_{l,j} x_l^k} A_{i,j} ,$$

where k is the number of iteration. 20-300 iteration is typical.

Parallelization & avoidance of multiply calculations

Update the i^{th} voxel in the k^{th} iteration:

$$x_i^{k+1} = x_i^k \frac{1}{\sum_j A(i,j)} \sum_j \frac{y_j}{\sum_l A(l,j) x_l^k} A(i,j)$$

↓

$$x_i^{k+1} = x_i^k N_i \sum_j \frac{y_j}{\sum_l A(l,j) x_l^k} A(i,j)$$

Pre-calculate the normalization of the i^{th} voxel:

$$N_i = \frac{1}{\sum_j A(i,j)}$$

Parallelization & avoidance of multiply calculations

Update the i^{th} voxel in the k^{th} iteration:

$$x_i^{k+1} = x_i^k N_i \sum_j \frac{y_j}{\sum_l A(l,j)x_l^k} A(i,j)$$

⇓

$$x_i^{k+1} = x_i^k N_i R_i^k$$

$R_i = 0$. For i^{th} voxel and j^{th} proton history:

$$R_i^k + = \frac{y_j}{\sum_l A(l,j)x_l^k} A(i,j)$$

Parallelization & avoidance of multiply calculations

Update the i^{th} voxel in the k^{th} iteration:

$$x_i^{k+1} = x_i^k N_i R_i^k$$

First: Calculate the Hadamard ratio (once per iteration):

$$H_j^k = \frac{y_j}{\sum_l A(l, j) x_l^k}$$

Second: $R_i = 0$. For i^{th} voxel and j^{th} proton history:

$$R_i^k += H_j^k A(i, j)$$

GPU algorithm

Algorithm 1 GPU algorithm

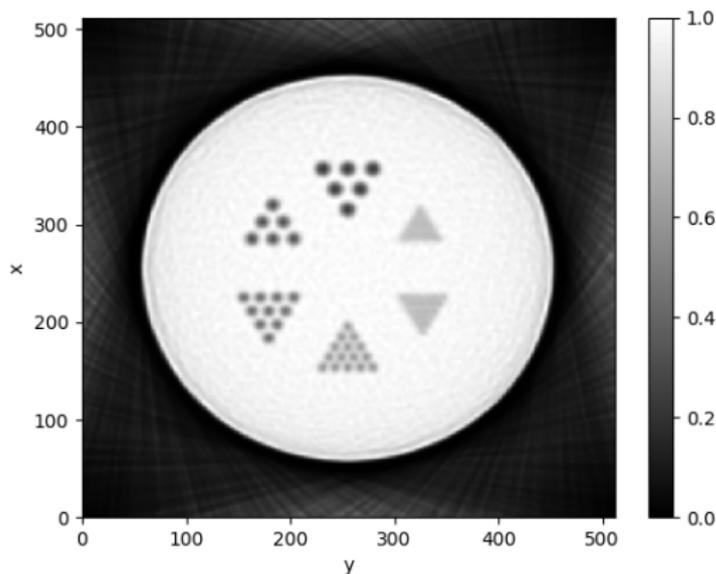
- 1: **GPU:** calculate voxel normalization
 - 2: **for** needed number of iterations **do**
 - 3: **while** end of proton histories **do**
 - 4: **CPU:** read certain amount of proton histories
 - 5: **GPU:** calculate Hadamard ratio:
 - parallel calculation of proton histories
 - serial calculation of voxel interactions
 - 6: **GPU:** calculate voxel contribution
 - serial calculation of proton histories
 - parallel calculation of voxel interactions
 - 7: **GPU:** Update the image vector
 - 8: **end while**
 - 9: **end for**
 - 10: **CPU:** Save the image vector
-

Results – reconstructed Derenzo phantom

Reconstructed Derenzo phantom after 250 iterations:

Derenzo phantom:

- For measurement of spatial resolution
- Group of rods in diameter distance
- Different diameters
⇒ test resolution



Results – reconstructed Derenzo phantom

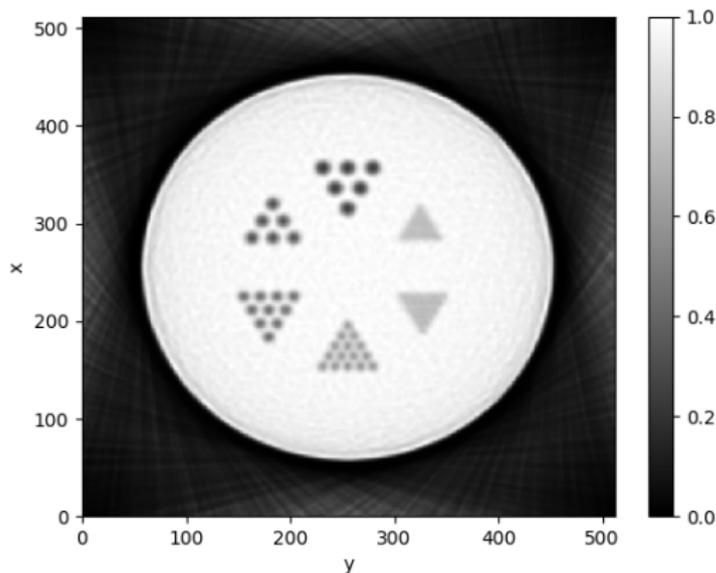
Reconstructed Derenzo phantom after 250 iterations:

Without errors:

- Exactly restored image

With errors:

- Reasonably good spatial resolution
- Point spread function FWHM = 4.3 mm
- Acceptable RSP accuracy



Summary

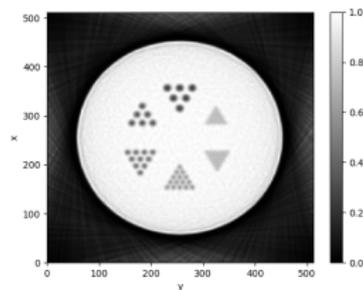
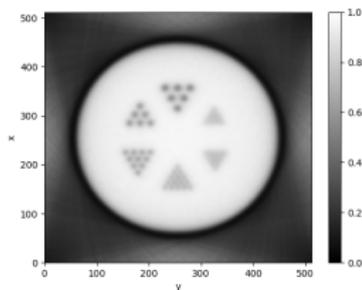
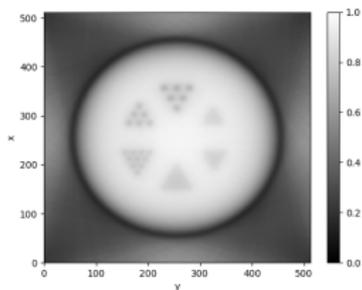
Results:

- A new development: statistically based pCT image reconstruction
- Application of Richardson–Lucy algorithm in pCT imaging
- Reasonably good resolution and acceptable RSP accuracy
⇒ promising from a first implementation of the algorithm

Outlook:

- Optimize the parameters & performance of the R–L algorithm
- New algorithm is based on Maximum Likelihood method

Thank you for your attention!



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